



Research Article

An experimental method of bioimpedance measurement and analysis for discriminating tissues of fruit or vegetable

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Abstract: It is difficult to apply bioimpedance technique to discriminate plant tissues due to the large variability of Cole parameters. A novel electronic method for characterizing tissue of fruit or vegetable with discrimination capability is presented. A specially designed electrode-pair is used to measure the bioimpedance and Cole parameters are extracted. The relaxation time which is a fundamental property of a given tissue is then estimated and analysis of variance is performed to gain statistical relevance. Bioimpedance is measured for apple and potato tissues in the frequency range of 1 Hz to 1 MHz and rigorous data analyses are performed. With 99% confidence, it is shown that the relaxation time is independent of position of measurement and is specific for a given fruit or vegetable. Further, the tissues of different species of a given fruit (or vegetable) is shown to be discriminated statistically at the confidence level of 98%. An excellent correlation is shown between the bioimpedance parameters and the parameters of cellular structure. Experimental data shows that our technique can be generalized to distinguish unhealthy or treated fruits (or vegetables) and therefore bearing immense applicability in the characterization of plant tissue.

Keywords: bioimpedance; Cole model; discrimination; electrical; measurement; tissue characterization

1. Introduction

The method of monitoring physiological condition by means of bioimpedance remains a novel technique for more than 50 years or so. The non-destructive method of bioimpedance measurement for fruits and vegetables is extensively used for various purposes such as to access health conditions [1,2], effect of storage conditions [3], physiological changes including assessing the quality of fruits and

vegetables [4–8]. On the other hand, investigations are also carried out to understand the science behind the characteristics of bioimpedance of plant tissues [9–17]

The necessity of invariability of bioimpedance parameters is extremely important in practical application of Cole model for discriminating fruits (or vegetables) from a reference fruit (or vegetable). Say for example someone wants to compare the Cole parameters for two different species of a given fruit. In such cases, the parameters can be compared if the parameters are not dependent on position (of a given fruit or sample). If the position (of measurement) dependent variability is high, one cannot distinguish two different samples under investigation. Thus, the measurement method should be robust enough to establish invariability of bioimpedance parameters which can be treated as reference parameters for comparison purpose.

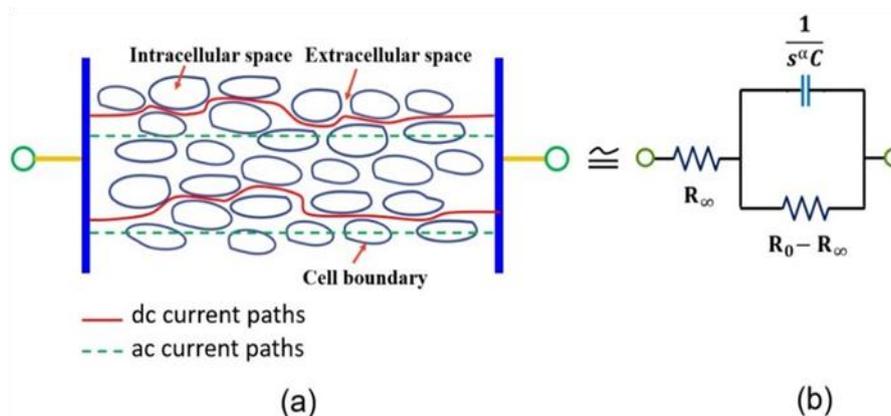


Figure 1. This figure is not in a scale. (a) Schematic of biological tissue. Straight dashed horizontal lines (green) represent the ac current path while the curvy lines (red) represent dc current path in biological tissue. (b) Cole equivalent circuit of lump tissue. Here, R_0 and R_∞ are the high and low frequency resistances respectively. C is the fractional capacitance and α ($0 < \alpha \leq 1$) is the dispersion (nonideality factor) parameter. The equivalent circuit consists of single dispersion parameter α .

Cole model is widely applied for living biological tissue [15,18–21]. In general, lump tissue is represented by Cole equivalent circuit and single dispersion model is accepted for its simplicity [7,14] (Figure 1). Among the various method of bioimpedance measurements, direct measurement (i.e. using LCR meter) with two-electrode configuration is the most generic one due to its high degree of reliability [5,20]. The electrical current paths inside a tissue is schematically shown in Figure 1 (a). It is intuitive from this figure, that if impedance is measured for the same tissue at other position, keeping the distance between the electrode invariant, one should obtain the same results (within the limits of experimental error for living tissue). On the other hand, if the distance between the electrodes is not kept same for measuring impedance at two different positions, the variability in measured parameters are clearly observed [14,15,22]. Thus, in order to obtain the comparable results among the samples, it is quite obvious to keep the distance between the electrode invariant. The reasons of choosing apple and potato are as follows. First of all, apple is a fruit whereas potato is a vegetable (tuber) and both of them are extensively used as food materials and therefore have importance in agriculture sector. Further, apple grows in open atmosphere whereas potato grows under soil. Not only these, the tissue

of apple will have a natural tendency towards ripen (or to be eaten) so that seed can be dispersed. On the other hand, potato tissue will have tendency to fight against external environment to sustain so as to produce the next generation potato. The porosity (fraction of empty space) of apple is highly different than that of potato.

In this work, a specific electrode-pair is designed and is used to measure bioimpedance of apple and potato tissues. It is needless to mention that, though apple is a fruit, potato is a vegetable and providing us two different kind of living tissue to be investigated under this study. Applying single dispersion Cole model, impedance parameters are extracted by curve fitting. It is established here that the tissue of apple and potato can be specified in terms of bioimpedance parameters which in turn can be used to discriminate similar tissue of different species with 98% confidence. Further, with 99% confidence, it is evidently shown here that the position of measurement of bioimpedance of a given fruit or vegetable is not a factor of variability. Thus, our process of measurement can directly be applied in assessing quality (or condition) of fruits or vegetables. In addition to this, our method can be applied to monitor the ripening of fruits similar to citrus fruit like orange [8].

2. Single dispersion Cole bioimpedance model

Single dispersion Cole bioimpedance model is a widely accepted model is extensively used for various kinds of biological tissue [5–8,10–21]. The single dispersion Cole equivalent circuit for lump biological tissue is shown in Figure 1(b). The equivalent circuit consists of a constant phase element (CPE) comprising of a fractional capacitor (C) with a parallel resistance ($R_0 - R_\infty$) and a series resistance R_∞ . The CPE maintains the phase invariacy by the dispersion parameter α . In the equivalent circuit, R_0 is the dc resistance (or low frequency resistance of the tissue); R_∞ is the ac resistance of tissue at high frequency. The impedance of single dispersion equivalent circuit (Cole equivalent circuit) is usually expressed as

$$Z = R_\infty + \frac{(R_0 - R_\infty)}{1 + (j\omega\tau)^\alpha} \quad (1)$$

where, $j = \sqrt{-1}$. The symbol τ in Eq. (1) is known as the characteristics time constant of the tissue and is expressed as

$$\tau = [(R_0 - R_\infty)C]^{1/\alpha} \quad (2)$$

Separation of Z into real and imaginary parts is not straight forward due to the non-integer value of α ($0 < \alpha \leq 1$), which turns the Eq. (1) into the category of fractional calculus. Nevertheless, analytically it is possible to express the impedance Z in terms of real and imaginary part using $j^\alpha = (j \sin \frac{\alpha\pi}{2} + \cos \frac{\alpha\pi}{2})$ and after simplifying we obtain

$$Z = X + jY \quad (3)$$

$$\text{where, } X = R_\infty + \frac{(R_0 - R_\infty)(1 + \omega^\alpha \tau^\alpha \cos \frac{\alpha\pi}{2})}{(1 + \omega^\alpha \tau^\alpha \cos \frac{\alpha\pi}{2})^2 + (\omega^\alpha \tau^\alpha \sin \frac{\alpha\pi}{2})^2} \text{ and } Y = - \frac{(R_0 - R_\infty)(\omega^\alpha \tau^\alpha \sin \frac{\alpha\pi}{2})}{(1 + \omega^\alpha \tau^\alpha \cos \frac{\alpha\pi}{2})^2 + (\omega^\alpha \tau^\alpha \sin \frac{\alpha\pi}{2})^2} .$$

Thus, the modulus of Z becomes

$$|Z| = \sqrt{\left(R_{\infty} + \frac{(R_0 - R_{\infty})(1 + \omega^{\alpha}\tau^{\alpha} \cos\frac{\alpha\pi}{2})}{(1 + \omega^{\alpha}\tau^{\alpha} \cos\frac{\alpha\pi}{2})^2 + (\omega^{\alpha}\tau^{\alpha} \sin\frac{\alpha\pi}{2})^2}\right)^2 + \left(\frac{(R_0 - R_{\infty})(\omega^{\alpha}\tau^{\alpha} \sin\frac{\alpha\pi}{2})}{(1 + \omega^{\alpha}\tau^{\alpha} \cos\frac{\alpha\pi}{2})^2 + (\omega^{\alpha}\tau^{\alpha} \sin\frac{\alpha\pi}{2})^2}\right)^2} \quad (4)$$

Experimentally, Eq. (4) $|Z|$ is obtained as a function of frequency $f (= \omega/2\pi)$. The experimental data is then fitted (non-linear curve fitting) and values of R_0 , R_{∞} , C , α are obtained. From these parameters, the relaxation time τ is calculated using Eq. (2).

3. Specially designed electrode-pair

In general, the physiological parameters are non-repetitive and standard deviation is large. For example, if at identical condition, the cell size is measured for a given tissue, the variation of more than 20% is not uncommon while the grain size of a metallic conductor is measured, the result is found to be within the tolerance level (about 5% or so). The variation in cell size would therefore lead to a large variation in the tissue related parameters. Thus, it is extremely important to specify the tissue by means of Cole model parameters as well as relaxation time. On the other hand, it is essential to keep the distance (or gap) between the electrode-pair invariant. Intuitively, this is due to the fact that the Cole parameters (except α) are highly dependent on the gap between the electrodes. Hence, to discriminate tissues from one another, it is essential to obtain the invariability of impedance irrespective of measuring position (of tissue) of fruits or vegetable.

An electrode-pair is designed and fabricated for the purpose of bioimpedance measurement of fruit or vegetable. A schematic of the fabricated electrode-pair is shown in Figure 2. The depth of penetration and diameter of the electrodes are 1.5 cm and 0.28 mm respectively and these are maintained throughout this work unless otherwise stated. The electrodes are separated by plastic material (of negligibly low leakage current). The plastic holder of the electrode-pair is made by cutting a disposable syringe. The gap between the electrode is kept at 3 mm. For electrode material, stain-less steel is chosen for its inertness of reacting with any other materials and retain sufficient strength at low wire diameter.

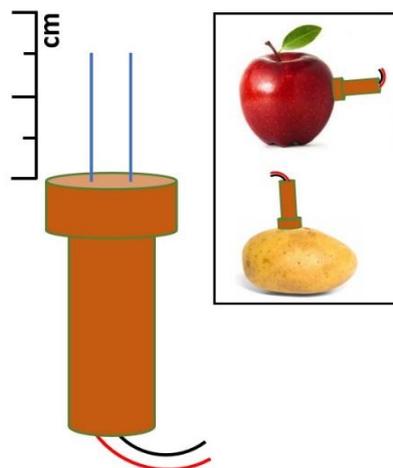


Figure 2. Schematic of electrode-pair. Typical pictures of accessing tissue of apple and potato using electrode-pair are shown in the inset of the Figure.

4. Experiments

Table 1. Sample matrix under study.

Sample	Species/Description	Designation of Measurement
Apple-1	Apple-1 and Apple-2 are of same species (Green Granny Smith) and both are purchased from same local shop. Apple-1 and Apple-2 can be considered to be biologically identical.	$A_{11}, A_{12}, A_{13}, A_{14}, A_{15}$
Apple-2		$A_{21}, A_{22}, A_{23}, A_{24}, A_{25}$
Apple-3	Apple-3 (Red Washington) is of different species that of Apple-1 and Apple-2. Apple-3 is biologically different from Apple-1 and Apple-2.	$A_{31}, A_{32}, A_{33}, A_{34}, A_{35}$
Potato-1	Potato-1 and Potato-2 are of same species (Kufri Chandramukhi) and both are purchased from same local shop. Potato-1 and Potato-2 can be considered to be biologically identical.	$P_{11}, P_{12}, P_{13}, P_{14}, P_{15}$
Potato-2		$P_{21}, P_{22}, P_{23}, P_{24}, P_{25}$
Potato-3	Potato-3 (Kufri Jyoti) is of different species that of Potato-1 and Potato-2. Potato-3 is biologically different from Potato-1 and Potato-2.	$P_{31}, P_{32}, P_{33}, P_{34}, P_{35}$

Remarks: In this table, A_{mn} (or P_{mn}) represents impedance measurement of Apple-m (or Potato-m) at position n.

The sample matrix is shown Table 1. In order to remove any parasitic effect that may arise from electrodes and probes, the LCR meter (Model: 8101G, Make: Gw Instek) is calibrated before taking any measurement data. Each time electrodes are cleaned by medicated sprit and dried properly before inserting into fruit or vegetable. By inserting the electrode-pair at desired position of the

sample, impedance is measured in the frequency range of 1 Hz to 1 MHz with amplitude of 1 V (peak to peak). All measurements are conducted at identical condition. In order to avoid any physical damage in the tissue due to high electric field, small signal is chosen for measurement. The impedance is found to decrease with the increase in frequency and becomes sufficiently flat around the frequency of 1 MHz and thus restricts the choice of upper limit on the frequency of interest. For each sample, five measurements are done at five different positions and each measurement contains four hundred data points. Typical measurement data are plotted as a function of frequency and is shown in Figure 3.

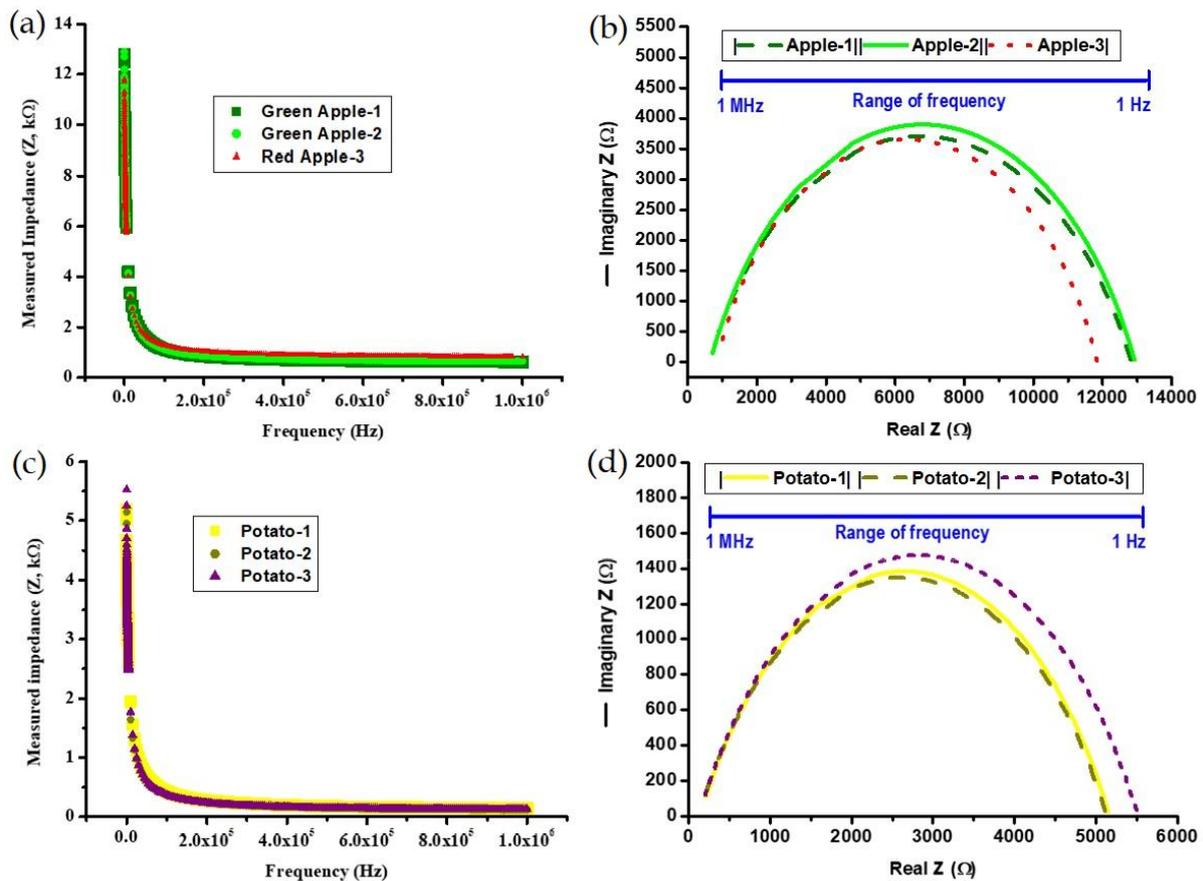


Figure 3. Measured tissue impedance as a function of frequency. (a) apple, (c) potato. Fitted Cole plots (b) apple, (d) potato.

5. Results and discussions

Experimentally $|Z|$ is obtained as a function of frequency for different samples and for different position of a given sample as mentioned in Table 1. The non-linear curve fitting is performed by commercial MS Excel 2016 package. As a common practice, in the curve fitting process, the value of R_0 and R_∞ is considered to be the measured values R_0 and R_∞ . Hence in this work, the measured impedances at 1 Hz and 1 MHz are considered to be R_0 and R_∞ respectively. The value of α and C are estimated by fitting the experimental curve with the Eq. (4). The characteristic time constant τ is then estimated using Eq. (2) for each set of data.

From the experimental plots of $|Z|$ as a function of frequency (see Figure 3) it is not possible to distinguish the species of a given fruit or vegetable and this is because the plots of different species almost overlap on each other when plotted simultaneously in a single graph. On the other hand, the important parameters related to equivalent circuit of these plots may differ significantly.

The fitted Cole plots are shown in Figure 3(b) and Figure 3(d) for apple and potato respectively. Since, the sample Apple-1 and Apple-2 are from same species, the Cole plots of these do not differ and follow one another for the entire span of frequency range. While the Cole plot for the sample Apple-3 slightly differ from the other two, especially at the low frequency range. This is probably due to the fact that the species of sample Apple-3 is different from that of sample Apple-1 or Apple-2. Exactly similar observation is found for potato samples (Figure 3. (d)). From the fitted Cole plots, it is noticed that the distinguishable capability of bioimpedance method is better at the low frequency range for apple as well for potato. This fact suggests that the bioimpedance study of apple and potato can be limited to 3 kHz. By reducing the frequency range while keeping the number data point same, we can obtain better experimental results.

5.1. ANOVA on apple and potato samples

In this study, all ANOVA are performed using commercial MS Excel 2016 package. The Cole parameters for apple samples are shown in Table 2. ANOVA on τ is performed considering position and sample as two factors. The first factor is considered to understand whether position of measurement is a factor or not. On the other hand, the second factor is considered to understand the discriminating capability of the bioimpedance measurement.

To test these hypotheses, two apples of same species (Green Granny Smith in this case) are taken from a local shop and thus the biological differences between the apples are minimized. Then for each apple, impedance is measured at five different positions. The measured and calculated data is shown in Table 2. Result of ANOVA for tissue of apple is shown in Table 3. Interestingly it is found that none of the factors are significant (since, $F_{critical} > F\text{-value}$) at the confidence level as high as 99% when ANOVA is performed among the sample Apple-1 and Apple-2. This means that one the Cole parameters i.e. the relaxation time are indistinguishable as far position is concerned. The two samples (Apple-1/Apple-2) are also found to be indistinguishable. Or in other words, the tissues of Apple-1 and Apple-2 are statistically same. Thus, with respect to our electrode system, the relaxation time is invariable and it does not depend on the position of measurement and remains same for biologically same samples.

On the other hand, though the position is found to be indistinguishable in Apple-1 and Apple-3 (or Apple-2 and Apple-3), they are found to be distinguishable ($F_{critical} < F\text{-value}$) when ANOVA is performed for these two pair of samples. Thus, again as before, the position of measurement is not found to be a factor. However, in the present two cases, the sample is found to be a factor and is discriminated by respective relaxation time. This means the tissues of Apple-1 and Apple-3 are different. This fact proves that the relaxation time of apple tissue can be used to discriminate different species of apple.

Table 2. Cole parameters obtained from experiment and curve fitting for apple.

Sample	R_0 (k Ω)	R_∞ (k Ω)	α	C (nF sec $^{\alpha-1}$)	τ (μ sec)	Regression coefficient
Apple-1	12.93	0.64	0.719	76.65	63	0.9989
	14.21	0.74	0.703	88.30	70	0.9987
	13.58	0.77	0.691	99.99	65	0.9983
	13.75	0.65	0.705	91.55	72	0.9989
	12.12	0.63	0.692	103.83	60	0.9983
Apple-2	12.83	0.61	0.694	98.25	63	0.9980
	13.67	0.70	0.708	86.55	69	0.9985
	13.90	0.72	0.696	103.47	76	0.9985
	12.47	0.67	0.693	112.05	70	0.9983
	10.97	0.70	0.694	113.46	59	0.9984
Apple-3	11.85	0.83	0.745	62.35	57	0.9993
	10.53	0.77	0.747	64.20	52	0.9991
	11.35	0.84	0.754	55.15	51	0.9994
	13.75	0.84	0.767	47.47	65	0.9997
	11.74	0.84	0.751	56.65	53	0.9993

Remarks: Apple-1&Apple-2 are of same species and are taken from same lot. While Apple-3 is different from the other two.

Table 3. Summary of ANOVA on τ for apple.

Sample	Factor	P-value	F-value	$F_{critical}$	Distinguishability	Level of Confidence
Apple-1 & Apple-2	Position	0.119	3.627	15.977	No	99%
	Sample	0.594	0.334	21.197	No	
Apple-1 & Apple-3	Position	0.146	3.153	10.899	No	98%
	Sample	0.017	15.384	14.039	Yes	

Table 4. Cole parameters obtained from experiment and curve fitting for potato.

Sample	R_0 (k Ω)	R_∞ (k Ω)	α	C (nF sec $^{\alpha-1}$)	τ (μ sec)	Regression coefficient
Potato-1	5.17	0.14	0.6400	341	48	0.9888
	5.48	0.16	0.7000	204	41	0.9956
	5.58	0.13	0.6638	246	47	0.9920
	5.65	0.12	0.6505	325	60	0.9922
	5.09	0.11	0.6797	243	51	0.9951
Potato-2	5.14	0.12	0.6275	445	60	0.9897
	5.43	0.13	0.6532	286	48	0.9918
	6.66	0.16	0.6077	450	68	0.9890
	4.70	0.12	0.6415	363	47	0.9891
	5.67	0.12	0.5979	580	68	0.9865
Potato-3	5.52	0.12	0.6360	420	70	0.9934
	5.57	0.15	0.6099	610	68	0.9906
	6.70	0.14	0.6202	432	78	0.9912
	5.86	0.11	0.6362	393	69	0.9916
	5.46	0.13	0.6436	349	57	0.9924

Remarks: Potato -1& Potato -2 are of same species and are taken from same lot, while Potato -3 is different from the other two.

Table 5. Summary of ANOVA on τ for potato.

Sample	Factor	P-value	F-value	$F_{critical}$	Distinguishability	Level of Confidence
Potato-1 & Potato-2	Position	0.6046	0.7537	15.977	No	99%
	Sample	0.2124	2.1975	21.198	No	
Potato-1& Potato-3	Position	0.6201	0.7218	10.899	No	98%
	Sample	0.0182	14.856	14.040	Yes	

The various Cole parameters for potato samples are tabulated in Table 4. Similar to apple

samples, ANOVA is performed on τ for potato samples and the result of the ANOVA is shown in Table 5. Based on the ANOVA, we have obtained similar conclusion as in apples. That is position of measurement is not a factor and different tissue of potato samples can be distinguished based on the relaxation time.

In order to gain confidence on our discrimination method described above, the entire experiment is repeated by taking another two specimens of each type using the same electrode-pair. When data is analyzed similar outcome is resulted. Thus, our method is found to be repetitive and robust.

5.2. Physiological difference between apple and potato

It is intuitive from the Figure 1(a), that the values of the Cole parameters are highly dependent on (a) cell size, (b) porosity, (c) constituents etc. In order to assess the cell size, extensive analysis is performed on the cellular images obtained using a confocal microscope (Olympus CX41). The average cell size of apple and potato (of typical species used in bioimpedance measurement) are estimated to be $(10\text{--}12) \times 10^3 \mu\text{m}^2$ and $(18\text{--}20) \times 10^3 \mu\text{m}^2$ respectively. The measured cell areas agree well with the similar measurement presented in published references [23,24]. Thus, the cell size of potato is about 1.8 times larger than that of apple.

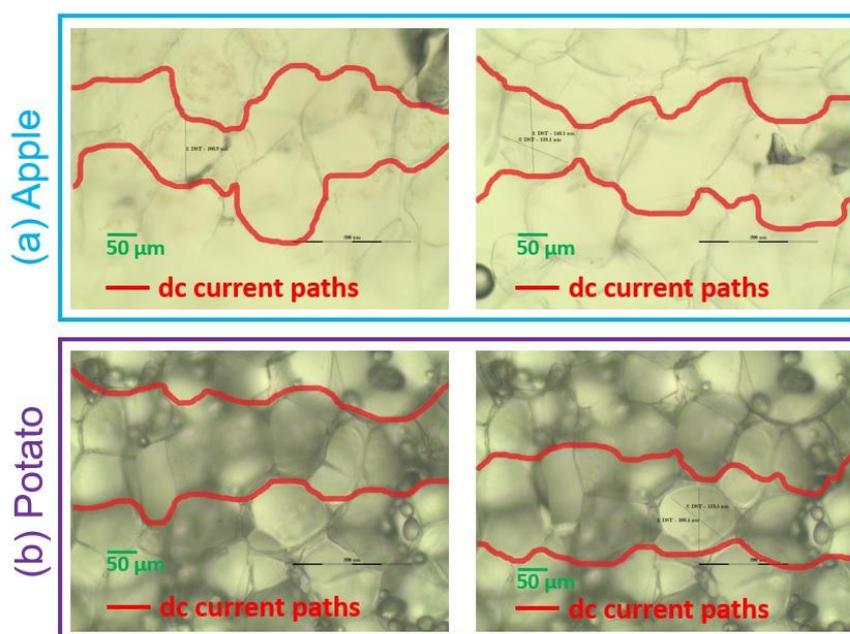


Figure 4. Images cellular structure of apple (top-left and top-right) and potato (bottom-left and bottom-right) obtained by confocal microscope (without any staining). The images are taken at the same scale for comparison purpose. Typical dc current paths are shown by dark detouring lines. The dc current paths are found to be longer in apple tissue in comparison to that of potato tissue.

On the other hand, the porosity of the apple and potato are in the range of 0.15–0.22 and 0.03–0.08 respectively [25]. Hence, apple tissue contains much more extracellular space than that of the potato.

The estimated cell size and porosity in the tissues under investigation can be used to explain the capacitance obtained experimentally. The capacitance of potato tissue is found larger than that of apple tissue (see Table II and Table IV). In the cellular structure, two nearby cells and extracellular space between cells behave like the plates and dielectric material respectively of a parallel plate capacitor. As the capacitance of a parallel plate capacitor is proportional to the plate area and is inversely proportional to the separation between the plates (the extracellular space), the capacitance (C) is found larger in potato tissue as its cell size is larger and extracellular space (porosity) is smaller.

The dc resistance on the other hand depends on the length the dc current path. Longer the dc current path, larger is the dc resistance R_0 . Typical dc current paths are drawn manually (based on the principle that dc current flows through the extracellular space) and are shown in Figure 4. It is clear from this figure that the detouring of dc current path of apple tissue is greater than that of potato tissue and as a result apple shows larger R_0 which is indeed found experimentally (see Table 2 and Table 4). Thus, the orientation of cells in the tissue highly affects the dc resistance. More the misorientation among the cells, longer is the dc current path and yields larger dc resistance. Another factor that may affect the dc resistance is the resistivity of the constituents of the extracellular space in tissues and such investigation is beyond the scope of this work. Therefore, the comparison of Cole parameters of the tissues of Apple and Potato from the biophysical point of view is tentative.

6. Conclusions

An experimental method is established here to distinguish different species of fruits or vegetable by means of measuring Cole parameters. Cole parameters are extracted for apple and potato tissue by specially designed electrode-pair using direct measurement technique. Among the various Cole parameters, the relaxation time τ is found to be most promising tissue characterizing parameter, since it contains all other Cole parameters of a given tissue. With statistical relevance, it is shown that tissues of different species of apple as well as potato can be distinguished by our experimental method. Our method can have wide application to distinguish unhealthy (or treated) fruits or vegetables from healthy one. The method is not costly and therefore this method has potential application in accessing plant tissue.

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Conflict of interest

The authors declare no conflicts of interest.

References

1. Greenham CG, Norris DO, Brock RD, et al. (1952) Some electrical differences between healthy and virus-infected potato tubers. *Nature* 169: 973–974.
2. Greenham CG, Helms K, Müller WJ (1978) Influence of virus inflections on impedance parameters. *J Exp Bot* 29: 867–877.
3. Greenham CG, Daday H (1957) Electrical determination of cold hardiness in *Trifolium repens* L. and *Medicago sativa* L. *Nature* 180: 541–543.
4. Jackson PJ, Harker FR (2000) Apple bruise detection by electrical impedance measurement. *HortScience* 35: 104–107.
5. Wu L, Ogawa Y, Tagawa A (2008) Electrical impedance spectroscopy analysis of eggplant pulp and effects of drying and freezing–thawing treatments on its impedance characteristics. *J Food Eng* 87: 274–280.
6. Jha SN, Narsaiah K, Basediya AL, et al. (2011) Measurement techniques and application of electrical properties for nondestructive quality evaluation of foods—a review. *J Food Sci Tech* 48: 387–411.
7. Khaled DE, Novas N, Gazquez JA, et al. (2015) Fruit and vegetable quality assessment via dielectric sensing. *Sensors* 15: 15363–15397.
8. Chowdhury A, Singh P, Bera TK, et al. (2017) Electrical impedance spectroscopic study of mandarin orange during ripening. *J Food Meas Charact* 11: 1654–1664.
9. Zhang MIN, Willison JHM (1993) Electrical impedance analysis in plant tissues. *J Exp Bot* 44: 1369–1375.
10. Grimnes S, Martinsen OG (2004) Cole electrical impedance model—a critique and an alternative. *IEEE T Biomed Eng* 52: 132–135.
11. Elwakil AS, Maundy B (2010) Extracting the Cole-Cole impedance model parameters without direct impedance measurement. *Electron Lett* 46: 1367–1368.
12. Freeborn TJ, Maundy B, Elwakil A (2011) Numerical extraction of Cole-Cole impedance parameters from step response. *Nonlinear Theory Appl, IEICE* 2: 548–561.
13. Freeborn TJ, Maundy B, Elwakil AS (2012) Least squares estimation technique of Cole-Cole parameters from step response. *Electron Lett* 48: 752–754.
14. Maundy BJ, Elwakil AS, Allagui A (2015) Extracting the parameters of the single-dispersion Cole bioimpedance model using a magnitude-only method. *Comput Electron Agr* 119: 153–157.
15. Freeborn TJ, Elwakil AS, Maundy B (2017) Variability of Cole-model bioimpedance parameters using magnitude-only measurements of apples from a two-electrode configuration. *Int J Food Prop* 20: S507–S519.
16. Freeborn TJ, Elwakil A, Maundy B (2016) Electrode location impact on cole-impedance parameters using magnitude-only measurements. *2016 IEEE 59th International Midwest Symposium on Circuits and Systems (MWSCAS)*, Abu Dhabi, United Arab Emirates.
17. Chowdhury A, Datta S, Bera TK, et al. (2018) Design and development of microcontroller based instrumentation for studying complex bioelectrical impedance of fruits using electrical impedance spectroscopy. *J Food Process Eng* 41: e12640.

18. Lingwood BE (2013) Bioelectrical impedance analysis for assessment of fluid status and body composition in neonates—the good, the bad and the unknown. *Eur J Clin Nutr* 67: S28–S33.
19. Kyle UG, Bosaeus I, De Lorenzo AD, et al. (2004) Bioelectrical impedance analysis—part I: review of principles and methods. *Clin Nutr* 23: 1226–1243.
20. Juansah J, Budiastra IW, Dahlan K, et al. (2014) Electrical properties of garut citrus fruits at low alternating current signal and its correlation with physicochemical properties during maturation. *Int J Food Prop* 17: 1498–1517.
21. Dovancescu S, Saporito S, Herold IHF, et al. (2019) Monitoring thoracic fluid content using bioelectrical impedance spectroscopy and Cole modeling. *J Electr Bioimpedance* 8: 107–115.
22. Arijit R, Pranay B, Abhishek M (2019) Identification of bioimpedance parameters for characterizing of tissue: a case study with apple tissue by ANOVA”, IEEE Int. *Conference on Sensor and Transducers*, Kolkata, India.
23. Cybulska J, Pieczywek PM, Zdunek A (2012) The effect of Ca^{2+} and cellular structure on apple firmness and acoustic emission. *Eur Food Res Technol* 235: 119–128.
24. Gancarz M, Konstankiewicz K (2007) Changes of cellular structure of potato tuber parenchyma tissues during storage. *Res Agr Eng* 53: 75–78.
25. Singh F, Katiyar VK, Singh BP (2015) Mathematical modeling to study influence of porosity on apple and potato during dehydration. *J Food Sci Tech* 52: 5442–5455.



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